EDGE DETECTION BASED ON AUGMENTED LAGRANGIAN METHOD FOR LOW- QUALITY MEDICAL IMAGES

VO THI HONG TUYET

Ho Chi Minh City Open University, Vietnam - tuyet.vth@ou.edu.vn

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ABSTRACT

Medical images are useful for the treatment process. They contain a lot of information on displaying abnormalities in your body. The contour of medical images is a matter of interest. In there, edge detection is a process prepared for boundaries. Therefore, the edge detection of medical images is very important. Other previous methods must sacrifice time for the accurate results. It is because the medical images in the real world have many impurities. In this paper, I propose a method of detecting edges in medical images which have impurities by using augmented lagrangian method to improve the Canny algorithm. My algorithm improves the ability to detect edges faster. Compared with other recent methods, the proposed method is more efficient.

Keywords: Augmented lagrangian method; Canny; Edge detection.

1. Introduction

When medical images have impurities, blur and noise details, the quality of them become worse. This is a big problem for the health professionals to diagnose a disease. Because the treatment processing is based on the information from medical images. They provide many details of an inside human body that naked eyes cannot see. The size or location of each part of a body changes with initial manifestation of diseases. The clearer the contours of an object (eg bone, liver, blood vessels, etc...) is, the higher the quality of medical images is. So detecting abnormalities accurately is very useful to maintain patients' lives. The detection of a body part is a process which combines pixels together, and it is called the edge detection. If an algorithm detects many edges, we will have more information about objects and we will be more comfortable in contour detecting or segmentation.

The principles of edge detection methods usually include removing the noise as a first step in this process (D. Marr, E. Hildreth, 1980). The quality of medical images is almost worse because of many reasons.The noised pixels which make the first step of edge detection don't get good results because of the presence of weak object in input images. Therefore, medical images which have weak objects become a big challenge for edge detection.

In the past, there are many algorithms which are proposed for edge detection, such as: Canny (John Canny, 1986), Sobel (O. R. Vincent and O. Folorunso, 2009), B-spline (Wang Yuping and Cai Yuanlong, 1995; A.D. Bhatt and R.V. Warkhedkar, 2008) or in the generation types of wavelet transform (Wang Yuping and Cai Yuanlong, 1995; Lei Zhang and Paul Bao, 2002; G. Easley, D. Labate, and W.Q. Lim, 2008). However, the previous methods are limited to weak objects. Wavelet transform could overcome the disadvantage, but the time processing is very long.

In this paper, I propose an algorithm for edge detection of objects in low-quality medical images. I present the basis of augmented lagrangian method and edge detection in section 2. The proposed method is presented in section 3. The results of experiments are compared with the ones of the recent methods in section 4. Finally, the

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conclusions are shown in section 5.

2. Augmented lagrangian method and edge detection method

2.1. Augmented lagrangian method

Image restoration is an algorithm which must recover the sharp image. In this process, the rehabilitation vector is a difficult problem. The idea of minimizing a total variation on optimization problem for spatial temporal data (Stanley H. chan, Ramsin Khoshabeh, Kristofor B. Gibson, Philip E. Gill and Truong Q. Nguyen, 2011) was proposed. They used an Augmented Lagrangian Method (ALM) to solve the constrained problem.

Α vector denoting the unknown (potentially sharp) image which has size M x N is called f (f $\in R^{MN \times 1}$). f is an ingredient of equation to find the observed image g, g $\in R^{MN \times 1}$. It is a linear shift invariant imaging system to calculate as:

$$g = Hf + \eta \tag{1}$$

where f is a vector denoting the unknown (potentially sharp) image of size M x N, g is a denoting the observed vector image, $\eta \in R^{MN \times 1}$ is a vector denoting the noise/blur, and the matrix $H \in R^{MN \times MN}$ is a linear transformation representing convolution operation.

TV/L1 (for minimization denoising TV/L2 image) minimization and (for deblurring image) were two problems mentioned in ALM (Stanley H. chan, Ramsin Khoshabeh, Kristofor B. Gibson, Philip E. Gill and Truong Q. Nguyen, 2011). They were defined as:

 $\underset{f}{\text{minimize}} \quad \frac{\mu}{2} \|Hf - g\|^2 + \|f\|_{TV}$

and

minimize
$$\mu \| Hf - g \|_1 + \| f \|_{TV}$$
 (3)

(2)

With the equations, µ is the regularization parameter. The authors were to find a saddle point of L(f, u, y). Then, they used the alternating direction method (ADM)

to solve f-subproblem, u-subproblem with TV/L2 and f-subproblem, u-subproblem and r-subproblem with TV/L1. The equation is:

$$\underset{f,u}{\text{minimize}} \frac{\mu}{2} \|\text{Hf-g}\|^2 + \|u\|_1 \qquad (4)$$
$$\underset{f,u}{\text{minimize}} \mu \|r\|_1 + \|u\|_1 \qquad (5)$$

and

subject to r = Hf - g and u = Df.

ALM (Stanley H. Ramsin chan. Khoshabeh, Kristofor B. Gibson, Philip E. Gill and Truong Q. Nguyen, 2011) can be summarized as follows:

(i) Input: vector denoting the observed image and convolution matrix, regularization parameter, the isotropic total variation.

(ii) Set parameter with value default. This step is depended on other types of TV/L1 or TV/I_2

(iii) Initialize the first value such as f, u.

(iv) Compute the matrices of the firstorder, forward finite difference operators along the horizontal, vertical and temporal directions.

(v) While not coverage do:

+ Solve the sub problems and update parameter.

+ Check convergence if false continue.

This proposed method is also used for video restoration. Because the truth of each video is still the sum of many images.

2.2. Edge detection method

The edge detection is a process which finds the connection between pixels. The connection depends on many reasons, such as distance, the colors between two different regions in an image, shadows, depth, texture, or surface color, etc. Sometimes, this process is also based on the important features of edges.

Edge is the boundary of regions in an image. Boundary may create many lines, corners, curves in an image because of intensity changes.

The definition of edge detection was proposed in 1980. The sequence includes smoothing, enhancement, detection and localization (D. Marr and E. Hildreth, 1980). The first step is the denoising for input images. The important requirement is to keep the features of edges when removing noise. Then, the authors uses filters to improve the quality of edges. The detection is the continued step, it is base on the values of threshold (the results of the previous step which are enhanced by filters). The finally step is the localization – based on the location of each edge.

The continuation of idea about edge detection, John Canny proposed Canny in 1986 with the name: "Α method computational approach to edge detection". In 1987, R. Deriche used Canny to derive a recursively implemented optimal edge detector. Canny method used Gaussian filter to smooth the image and applied double determine potential edges. threshold to That parallel, Sobel (O. R. Vincent and O. Folorunso, 2009) was based on the approximation values M_x and M_y:

	-1	0	1]			-1	-2	-1]
$M_x =$	-2	0	2		$M_{y} =$	0	0	0
	1	0	1	and	ŕ	1	2	1

B-spline was also detected for edges (Wang Yuping and Cai Yuanlong, 1995; A.D. Bhatt and R.V. Warkhedkar, 2008) or combined with Active contour Snakes (Patrick Brigger and Michael Unser, 1998). Other algorithms were detected in wavelet transform (Wang Yuping and Cai Yuanlong, 1995; Lei Zhang and Paul Bao, 2002). With transform, the authors proposed the detection based on the combination between pixels in domain. Edge detection is based on estimating the gradient: strength, gradient direction by -90 degrees. The gradient is the twodimensional equivalent of the first derivative and is defined as the vector.

3. Edge detection based on augmented lagrangian method to improve the results of Canny method

Every little detail of medical images is very important. Each detail is an area which is connected by edges. Therefore, the number of edge detection is very helpful for the treatment of specialists in this field. When ege detection exacts the contour of each part, the change of size, shape, etc... may be a manifestation of a disease.

Many methods based on the masks such as Sobel (O. R. Vincent and O. Folorunso, 2009) and the proposed method takes advantage of the structure in local images. Recently, the transform is continued to solve this problem (Wang Yuping and Cai Yuanlong, 1995; Lei Zhang and Paul Bao, 2002). But, with transform, images must be adapte for threshold and filter many times. That loses small details which are extremely precious in medical images. And applications take a lot of times. That doesn't yet mention that the main reason why medical images with noise make a weak object. The detection of noisy images by Canny has a stronger contour than Sobel because it tracks edge by hysteresis.

Canny algorithm (John Canny, 1986) includes 5 steps: smooth images - find the intensity - edge detection by non-maximum suppression - to determine potential edges track edges. It is similar to using threshold and filter in transform. The idea may lose the information of images because of applying double threshold to determine potential edges. The process is very complex by Gaussian filter and threshold.

In this paper, I accost Augmented Lagrangian Method (ALM) to improve the result of Canny method. My algorithm can be summarized as figure 1.



Figure 1. The proposed method

The smoothing image:

ALM uses minimization to remove the noise or blur details out of pixels. In here, my proposed method applies TV/L1 process which follows (Stanley H. chan, Ramsin Khoshabeh, Kristofor B. Gibson, Philip E. Gill and Truong Q. Nguyen, 2011):

$$minimize_{f,r,u} \ \mu \|r\|_1 + \|u\|_1 \tag{6}$$

(i) Input: vector denoting the observed image (g) and convolution matrix (H), regularization parameter μ , the isotropic total variation β_x , β_y , β_t .

(ii) Set parameter with value default for $\rho_r = 2$, $\rho_0 = 100(\rho_r \text{ is a regularization})$ parameter) and $\alpha_0 = 0.7$.

(iii) Initialize $f_0 = g$, $u_0 = Df_0$, $y_0 = 0$, $r_0 = Hf_0 - g$, $z_0 = 0$. (y is the Lagrange multiplier)

(iv) Compute the matrices of the firstorder, forward finite difference operators along the horizontal, vertical and temporal directions.

while (not coverage) do:

• Solve the f-subproblem is: $minimize_f = \frac{\rho_0}{2} ||r - Hf + g||^2 +$

$$\frac{\rho_r}{2} \|u - Df\|^2 + z^T Hf + y^T Df$$
(7)

where $D = \begin{bmatrix} D_x^T & D_y^T & D_t^T \end{bmatrix}^T$, D_x , D_y , D_t are the first – order forward finite-difference operators along the horizontal, vertical, and temporal directions.

f-subprobem is improved by equation:

$$f = \mathcal{F}^{-1} \left[\frac{\mathcal{F}[\rho_0 H^T g + H^T(\rho_0 r - z) + D^T(\rho_r u - y)]}{\rho_0 |\mathcal{F}[H]|^2 + \rho_r \left(|\mathcal{F}[D_x]|^2 + |\mathcal{F}[D_y]|^2 + |\mathcal{F}[D_t]|^2 \right)} \right]$$
(8)

where \mathcal{F} denotes the three-dimensional Fourier Transform operator.

• Solve the u-subproblem is:

$$u_{k+1} = \arg\min_{u} ||u||_{1} - y_{k}^{T}(u - Df_{k+1}) + \frac{\rho_{r}}{2} ||u - Df_{k+1}||^{2}$$
(9)
by equation:

$$u_x = \max\left\{ \left| v_x \right| - \frac{1}{\rho_r}, 0 \right\} * sign(v_x)$$
 (10)

$$\begin{array}{l} \mininimize_{r} \ \ \mu \|r\|_{1} - z^{T}r + \\ \frac{\rho_{0}}{2} \|r - Hf + g\|^{2} \end{array} \tag{11}$$

by equation:

$$r = max \left\{ \left| Hf - g + \frac{1}{\rho_0} z \right| - \frac{\mu}{\rho_0}, 0 \right\} *$$

sign $\left(Hf - g + \frac{1}{\rho_0} z \right)$ (12)

• Update the Lagrange multiplier y and z:

$$y_{k+1} = y_k - \rho_r (u_{k+1} - Df_{k+1})$$
(13)
and

$$z_{k+1} = z_k - \rho_0 (r_{k+1} - Hf_{k+1} + g)$$
 (14)
• Update:

$$\boldsymbol{\rho}_{r} = \begin{cases} \gamma \rho_{r}, if \|\boldsymbol{u}_{k+1} - Df_{k+1}\|_{2} \ge \alpha \|\boldsymbol{u}_{k} - Df_{k}\|_{2} \\ \rho_{r}, otherwise \end{cases}$$
(15)

• Check convergence: if

 $\|f_{k+1} - f_k\|_2 / \|f_k\|_2 \le tol$ then break *end while.*

• To determine potential edges and track edges:

After the smoothing step by ALM, determining gradients of the medical images is also known as the edge strengths. This value is calculated by Euclidean distance measure, and it will be used to define edges to be shown. Euclidean distance can be calculated by:

$$E = \left(\sum_{i=1}^{n} |x_i - y_i|^2\right)^{1/2}$$
(16)

where x and y are the coordinates of image pixels.

Nonetheless, these edges will be converted to "sharp" edges in the nonmaximum suppression step. In each pixel of the gradient image, the gradient direction $< 45^{0}$ and 8-connected neighborhoods are mentioned. The direction of edges is shown by equation:

$$\theta = \arctan\left(\frac{|G_y|}{|G_x|}\right) \tag{17}$$

where G_x and G_y are the gradients in the x and y directions respectively.

If the edge strength between 8-connected neighborhoods, it will be removed. From the shown edges, the weak objects are improved by denoising with ALM and non-maximum suppression step. Thus, the number of strong objects is higher.

The hysteresis processing is to check the existence of weak edges in edge detection of

medical images. Because the weak edges are always the components in strong edges combined with 8-connected neighborhoods when they are tracked. So, the weak edges will be presented in the detected results.

Finally, the results have many useful details. Here is the success of Canny; and it is continued in my algorithm. The time processing is shortene by ALM in the first step. The proposed method doesn't use double threshold and filter to remove noise. That is to avoid the information of medical images when they are detected.

4. Experiments and results

As mentioned in section 3, this paper improves the quality of Canny algorithm by ALM to remove noise at the smoothing step. The idea is to remove the usage of double threshold and filter of the previous Canny method. On the other hand, the proposed method also saves execution time. Because the time processing of other methods, using transform or combined threshold, is very slow.

The experiments were tested on different noise and blur levels of additive and multiplicative noise. My data set is a set of images which includes many types of medical images, such as CT, MRI, etc... This data set is free and available at http://www.barre.nom.fr/medical/samples/.

Two cases of strong and weak objects were tested; the size of testing images is 256x256. Each case calculated the number of edges which appears in the result image, and the time processing of each method. The results of my proposed method are compared with other methods such as Canny (John Canny, 1986), Cuckoo Search (Gonzalez, C.I., Castro, J.R., Melin, P. and Castillo, O, 2011) and the scale multiplication wavelet transform (Lei Zhang and Paul Bao, 2002). The proposed method has more edges than other methods, but the time processing is shorter.



Figure 2. The results of edge detection by other methods with strong object in medical image

- (a) The strong object in the original medical image.
- (b) Edge detection by Canny method (3539 edges, execution time ~ 1500 seconds)
- (c) Edge detection by Cuckoo search method (3603 edges, execution time ~ 1850 seconds)
- (d) Edge detection by the scale multiplication wavelet transform (3745 edges, execution time ~ 3700 seconds)
- (e) Edge detection by the proposed method (3879 edges, execution time ~ 1900 seconds)

In this case, figure 2(a) shows the original medical image. The results of Canny for edge detection are illustrated in figure 2(b), the results of Cuckoo search are illustrated in figure 2(c), the results of scale multiplication wavelet transform are illustrated in figure 2(d). Figure 2(e) shows the results of our proposed method. We can see the edge detection by the proposed method is better than the results shown in figure 2(b), 2(c) and 2(d).





- (a) The weak object in the original medical image.
- (b) Edge detection by Canny method (1905 edges, execution time ~ 1700 seconds)
- (c) Edge detection by Cuckoo search method (2973 edges, execution time ~ 2200 seconds)
- (d) Edge detection by the scale multiplication wavelet transform (3236 edges, execution time ~ 4500 seconds)
- (e) Edge detection by the proposed method (4359 edges, execution time ~ 2100 seconds)

In Figure 3, the medical image which has a weak object was tested. In Figure 3(a), the original medical image has a weak object. It is an object with boundaries which are blurred and noised. Nevertheless, the blur is a problem easily overcome by technical skill or the quality of machine. The noise details are more popular than blur details. In this case, Gaussian noise and blur are added to medical images with the variance noise that is 0.00005 and the values of point spread the function of Gaussian blur. The reason why Gaussian is selected with the plus noise and blur into pixels of medical images. They are very popular in medical images.

The results of Canny for edge detection are illustrated in figure 3(b), the results of Cuckoo search are illustrated in Figure 3(c), the results of scale multiplication wavelet transform are illustrated infigure 3(d). Figure 3(e) shows the results of our proposed method. We can see the edge detection by the proposed method is better than the results shown in Figure 3(b), 3(c) and 3(d).

From the results from Figure 2, Figure 3 and many other test cases, I conclude that the results of the proposed method are better than Canny, Cuckoo search and the scale multiplication wavelet transform in two cases: strong object and weak object. The number of edge detection which can be seen by naked eyes is higher than other methods. This paper proposes another evaluation which is to count the number of edges. This evaluation returns to the number of nonzero elements in image matrix. The execution time of the proposed method is longer than Canny and Cuckoo search methods, but shorter than transform shown in figure (d).

In edge detection for medical images, to avoid the loss of information, algorithm should not use filter or threshold to remove bad pixels. My proposed method improves the quality of the boundaries by threshold in the first step of Canny, make them smoothier and give more information than transform or multithreshold. If the relationship between neighborhood and pixel, the edge strength, is not the largest, the algorithm can be removed. However, I can consider it if the strength is larger than over eight connected neighborhood.

5. Conclusion

The adaptation of threshold and filter has many difficulties for image processing. This is a big problem for denoising or deblurring algorithms. Any denoising and deblurring methods successful, it is the good premise for edge detection, contour or segmentation. The higher the number of edge detection is, the better the result of contour or segmentation is. In this paper, I propose a method to strengthen the quality of weak objects in order to improve the results of edge detection. My idea is to reconstruct the medical images which have noise and blur. The idea is based on augmented lagrangian method to improve the results of Canny method. The results of the proposed method are compared with other methods such as Canny (John Canny, 1986), Cuckoo Search (Gonzalez, C.I., Castro, J.R., Melin, P. and Castillo, O, 2011) and the scale multiplication wavelet transform (Lei Zhang and Paul Bao, 2002). The results shows that the proposed method detects more edges than other methods

References

- Brigger, P. & Unser, M. (1998). Multi-scale B-spline Snakes for General Contour Detection. Wavelet Applications in Signal and Image Processing VI, SPIE, 3458.
- Bhatt, A.D. & Warkhedkar, R.V. (2008). Reverse engineering of human body: a B-Spline based heterogeneous modeling approach. *Computer-Aided Design and Applications*, 5(1-4), 194-208.
- Bhatt, A.D. & Warkhedkar, R.V. (2009). Material-solid modeling of human body: a heterogeneous B-Spline based approach. *Computer-Aided Design*, *41*, 586-597.
- Canny, J. (1986). A computational approach to edge detection. *Pattern Analysis and Machine Intelligence, IEEE Transactions on, PAMI*, 8(6), 679-698.

- Deriche, R. (1987). Using Canny's criteria to derive a recursively implemented optimal edge detector. Int. J. Computer Vision, 1, 167-187.
- Easley, G., Labate, D. & Lim, W.Q. (2008). Sparse directional image representations using the discrete shearlet transform. *Appl.Comput. Harmon. Anal.*
- Gonzalez, C.I., Castro, J.R., Melin, P., & Castillo, O (2015). Cuckoo search algorithm for the optimization of type-2 fuzzy image edge detection systems. *Evolutionary Computation (CEC), IEEE Congress on*, 449-455.
- Marr, D. & Hildreth, E. (1980). Theory of edge detection. Proc. Royal Society, London, 187-217.
- Srishti (2014). Technique Based on Cuckoo's Search Algorithm for Exudates Detection in Diabetic Retinopathy. *Ophthalmology Research: An International Journal, SCIENCEDOMAIN international, 2*(1), 43-54.
- Strang, G. (1989). Wavelets and dilation equations. A brief introduction. SIAM Review, 31(4).
- Stanley, H., Khoshabeh, R., Kristofor, B. Gibson, Philip, E. Gill & Truong Q. Nguyen (2011). An Augmented Lagrangian Method for Total Variation Video Restoration. *IEEE Trans. Image Process*, 20(11), 3097-3111.
- Vincent, O.R. & Folorunso, O. (2009). A Descriptive Algorithm for Sobel Image Edge Detection. Proceedings of Informing Science & IT Education Conference (InSITE).
- Yuping, W. & Yuanlong, C. (1995). Multiscale B-spline wavelet for edge detection. *Science in China (Series A)*, 38(4).
- Zhang, L. & Paul Bao (2002). Edge detection by scale multiplication in wavelet domain. Pattern Recognition Letters 23, Elsevier, 1771-1784.